Brain Tumor Detection and Classification using Novel Image Segmentation Approach for MRI Images

Research Scholar

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Guide

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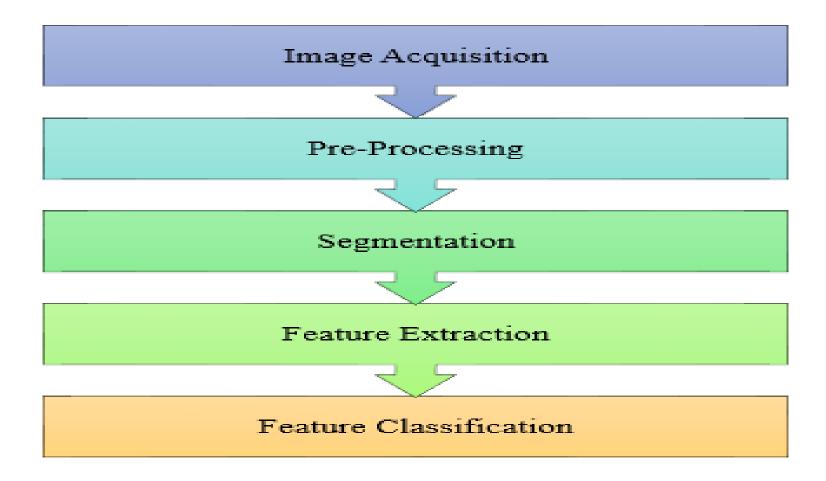


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1. MOTIVATION AND INTRODUCTION

- High risk factor with abnormal growth of brain tumor cells
- Brain tumor detection and classification is highly recommended for medical diagnosis and treatment
- Machine learning approach for brain tumor detection and classification
- Modalities (MRI, CT scan, etc.)
- Types of Tumors Benign and Malignant

2. GENERAL BLOCK DIAGRAM OF THE IMAGE DETECTION AND CLASSIFICATION



3. LITERATURE REVIEW

1) Image Modalities

- ➤ CT-Scan [5,18]
- ≻ X-RAY [5,18]
- ➤ MRI [5,18,19,20,21]
- 2) Pre-Processing
 - Gaussian Noise
 - Median Filter [1,2,23,25,34]
 - Wiener Filter [1,2,34,39]

Salt and Pepper Noise

- Median Filter [1,2,23,24,25,34]
- Speckle Noise
 - Anisotropic Filter [35,40,45,49]
 - Non Local Means Filter [8,9,10,26,50]
- Rician Noise
 - Wiener Filter [1,2,39]
- 3) Segmentation

Region Based method, Edge Detection, Clustering, Thresholding [6,53,54]

Multi-Thresholding [5,29]

- Particle Swarm Optimization algorithm [7,50,46,47]
- Harmony Search Algorithm[28,37]
- Differential Evolution Algorithm [36]
- Cuckoo Search Algorithm [4,10,11,12,13,14,41,48]

4) Feature Extraction

- Discrete Wavelet Transform [16,30,38,44,42]
- ➢ Gray Level Co-occurance Matrix [3,22,30,42,43]
- Local Binary Pattern [30,32,43,50]

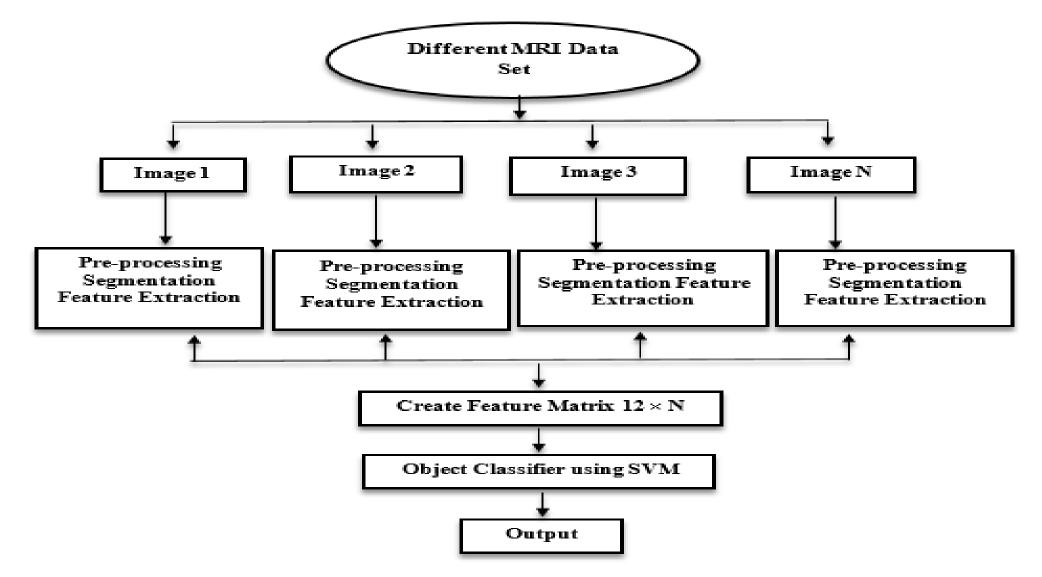
5) Classification

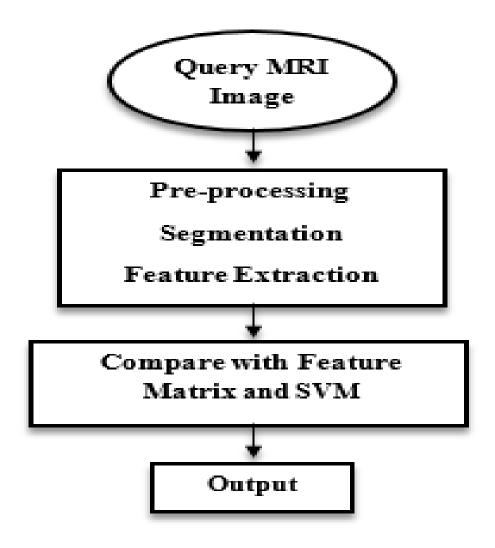
- Support Vector Machine [3,17,27,31,32]
- Random Forest [27,52]
- ➤ K Nearest Neighbour [27,33]

4. OBJECTIVE

- The objective of brain tumor detection is to create a software model that is capable of accurately predicting and categorizing tumors based on MRI images.
- With software algorithm, brain tumor prediction will be executed very quickly with high accuracy which assist doctor to recommend treatment for patients.

5. BRAIN TUMOR DETECTION AND CLASSIFICATION



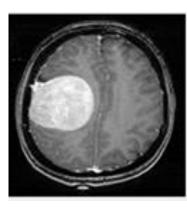


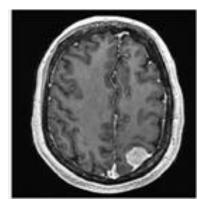
➢All the algorithms are implemented in Software and executed on the Core i3, 1.73GHz CPU with 512 GB hard disk. Image Processing toolbox, Wavelet Toolbox, etc available in Software.

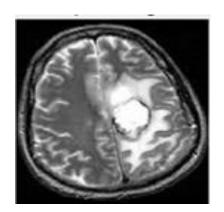
1) Image Dataset:

A) kaggle dataset (www.kaggle.com)

• 600 brain images, 400 tumor images, 200 without tumor images

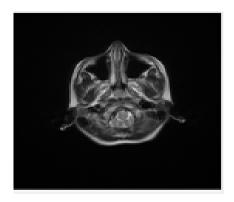


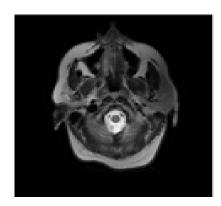


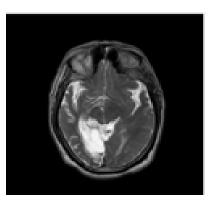


B) Sahyog Imaging Centre, SSG Hospital, Baroda Medical College, The Maharaja Sayajirao University of the Baroda, Vadodara, Gujarat, India

- 50 patients data, 30 males and 20 females patients
- 450 brain tumor images, 250 no tumor images







2) Pre-Processing:

Wiener Filter

x(m, n) - degraded input image, X(u, v)- Discrete Fourier Transform of x(m, n), $\hat{S}(u, v)$ - estimated value of the input image.

$$\hat{S}(u,v) = W(u,v) X(u,v)$$

The Wiener filter is defined as,

$$W(u,v) = \frac{H^*(u,v)}{|H(u,v)|^2} + \frac{P_n(u,v)}{P_s(u,v)}$$

H(u, v) - Fourier transform of the point spread function (PSF)

 P_s (u, v)- Power spectrum of the signal process, generated by the application of the Fourier transform of the signal autocorrelation

 $P_n(u,v)$ - Power spectrum of the Gaussian noise process, generated by the application of the Fourier transform of the noise autocorrelation

The inverse Fourier Transform of $\hat{S}(u, v)$, got the output(restored image).

Median Filter

 $Q(i,j) = median \{I(s,t)\}, where (s,t) \in M_{ij}\}$

where Q is output image, I is the input image and M_{ii} (window/mask).

*****Anisotropic Filter

 $I_t = div(c(x, y, t), \nabla I)$ $c(x, y, t) = g(\|\nabla I(x, y, t)\|)$

Where, div is the divergence operator, ∇ is the gradient, $|\nabla I|$ represents the magnitude of gradient

$$I_{i,j}^{t+1} = I_{i,j}^{t} + \lambda [c_{N}, \nabla_{N}I + c_{S}\nabla_{S}I + c_{E}\nabla_{E}I + c_{W}\nabla_{W}I]_{i,j}^{t}$$
The symbol ∇ indicates nearest-neighbour differences:

$$\nabla_{N}I_{i,j} = I_{i-1,j} - I_{i,j}$$

$$\nabla_{E}I_{i,j} = I_{i,j+1} - I_{i,j}$$

$$\nabla_{W}I_{i,j} = I_{i,j-1} - I_{i,j}$$

$$c_{Si,j}^{t} = g(\nabla_{N} I_{i,j}^{t})$$

$$c_{Si,j}^{t} = g(\nabla_{N} I_{i,j}^{t})$$

$$c_{Ei,j}^{t} = g(\nabla_{E} I_{i,j}^{t})$$

$$c_{Wi,j}^{t} = g(\nabla_{W} I_{i,j}^{t})$$

For High contrast edges over low contrast ones, $g(\nabla I) = e^{\left(\frac{\|\nabla I\|}{K}\right)^2}$ For wide regions over smaller ones, $g(\nabla I) = \frac{1}{1 + \left(\frac{\|\nabla I\|}{K}\right)^2}$, K=constant and $0 \le \lambda \le \frac{1}{4}$

Non Local Means Filter

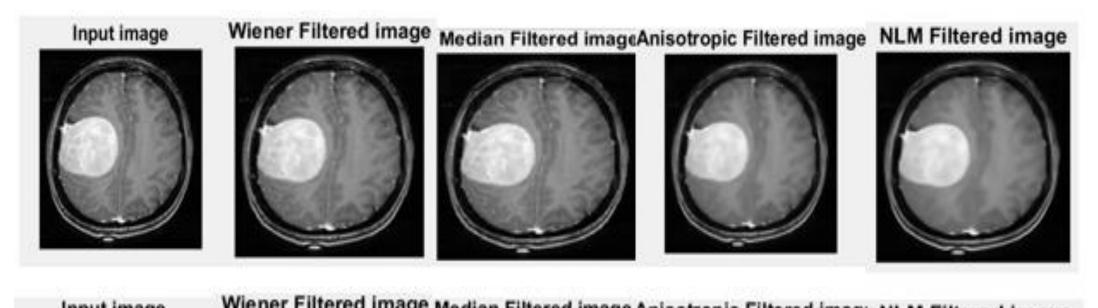
In a noisy image, $n = \{n(i) \mid i \in I\}$, the projected result NL(n)(i) is quantified as a weighted mean of entire pixel of scan,

$$NL(n)(x_i) = \sum_{j \in I} q(x_i, x_j) n(x_j)$$

 $q(x_i, x_j)$ indicates the weight assigned to $n(x_j)$ in attempt to recreate the pixel x_i and computed as:

$$q(x_i, x_j) = \frac{1}{Z_i} e^{\left(-\frac{(n(I)_i - n(I)_j)^2}{h^2}\right)}$$

 I_i and I_j are the intensities of regional area foci on pixels x_i and x_j , Z_i is the standardization variable, and h is the filtration parameter



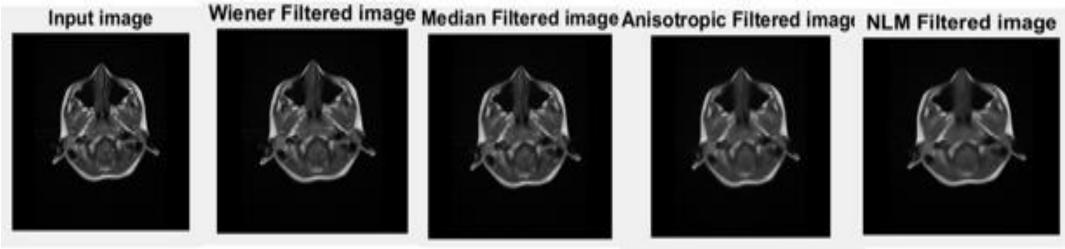


Figure-1: Implementation of different pre-processing filtering algorithms

Statistical parameters

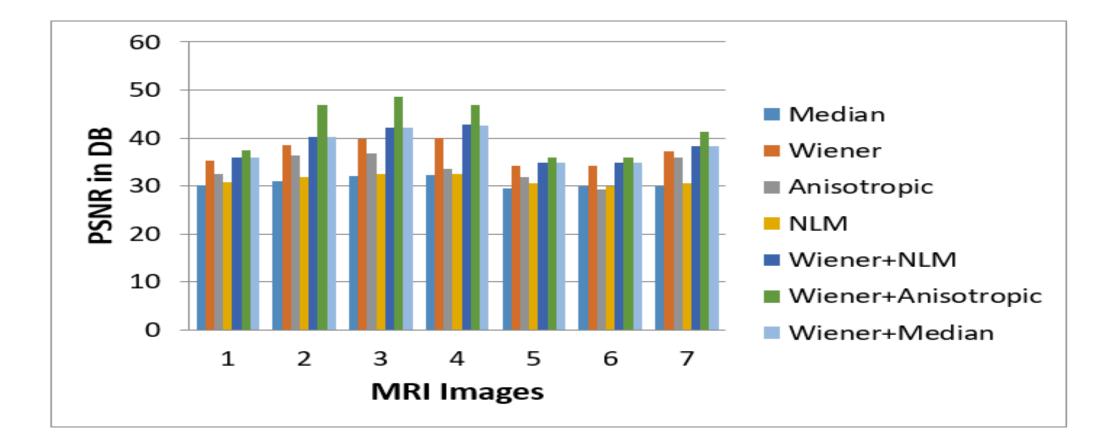


Figure-2: PSNR of the Brain Images after applying different filtering techniques

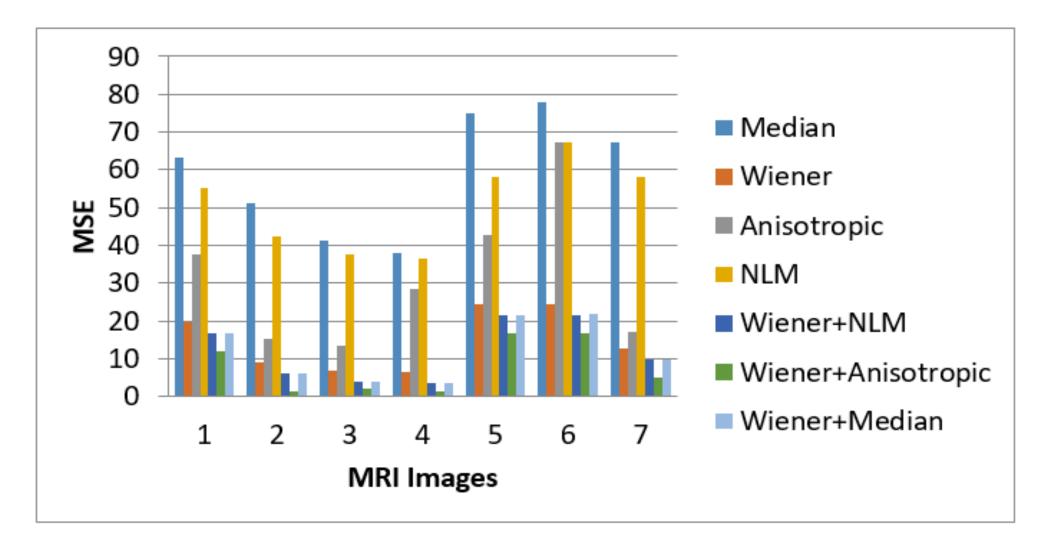


Figure-3: MSE of the Brain Images after applying different filtering techniques

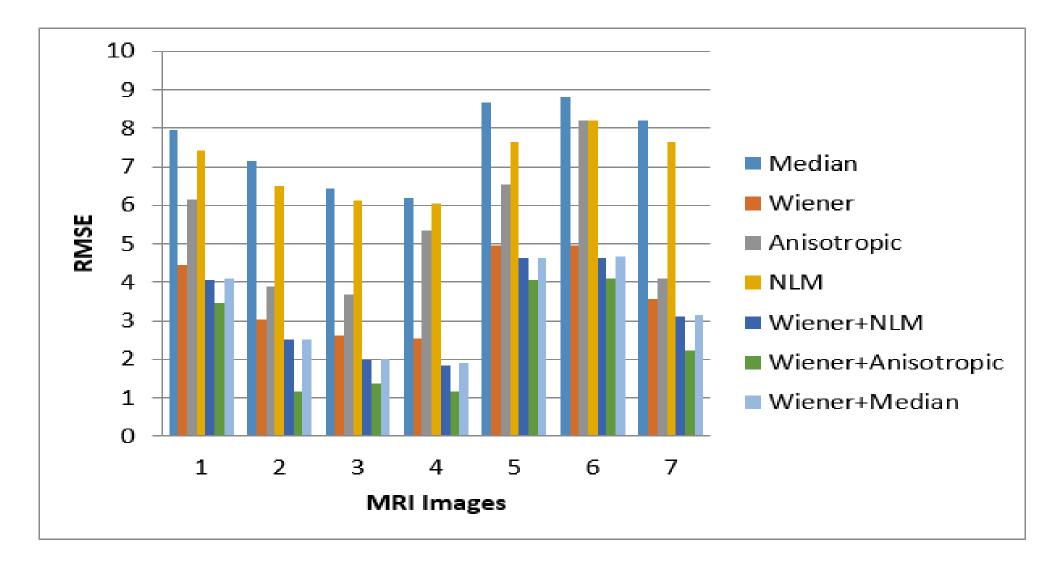


Figure-4: RMSE of the Brain Images after applying different filtering techniques

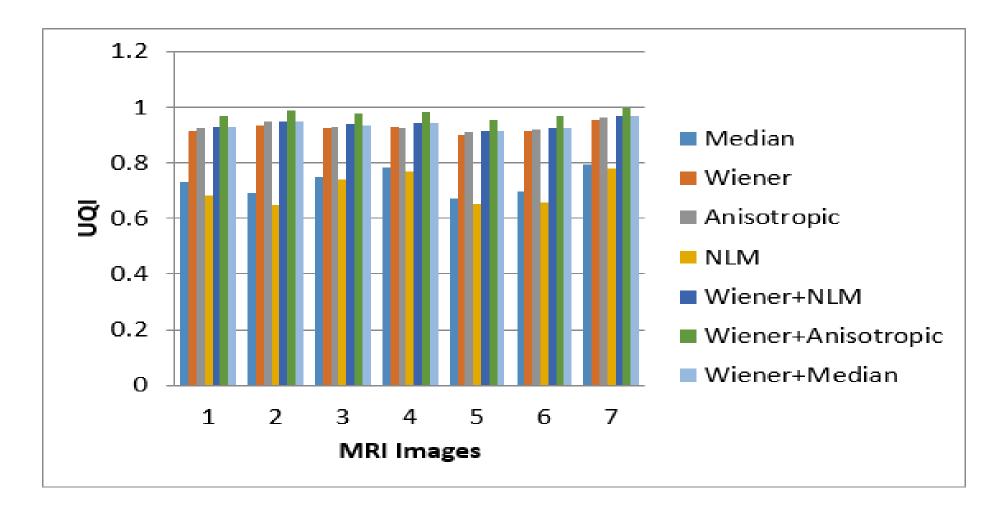


Figure-5: UQI of the Brain Images after applying different filtering techniques

Anisotropic Filtered image Wiener Filtered image Median Filtered image Input image NLM Filtered image Wiener + NLM Filtered image Wiener + Anisotropic Filtered image Wiener + Median Filtered image

Figure-6: Implementation of different pre-processing filtering algorithms

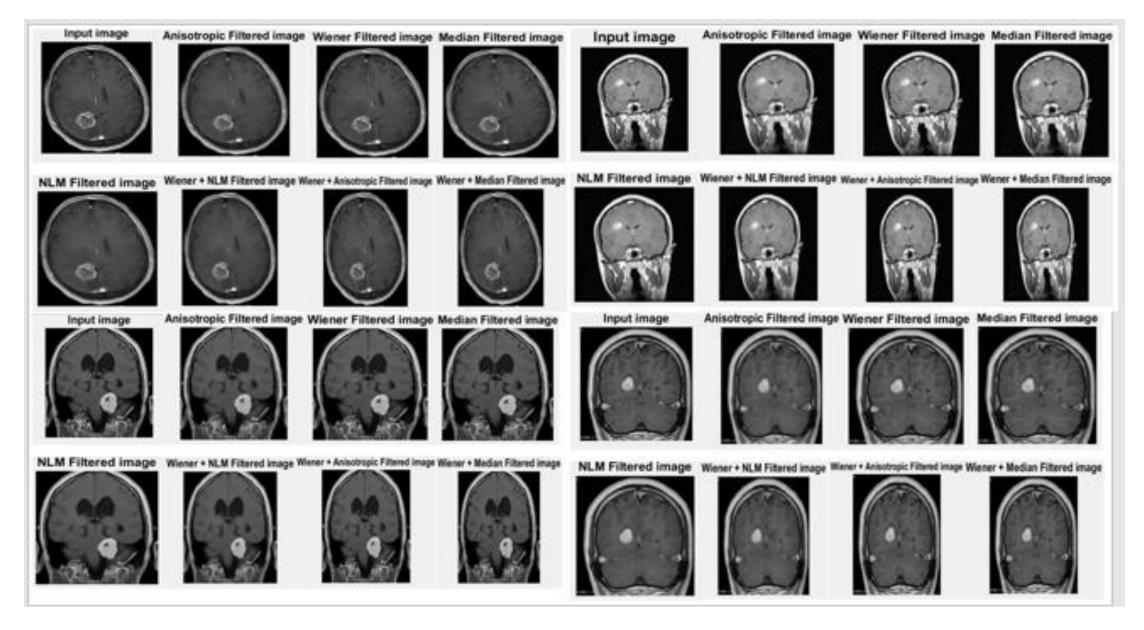


Figure-7: Implementation of different pre-processing filtering algorithms

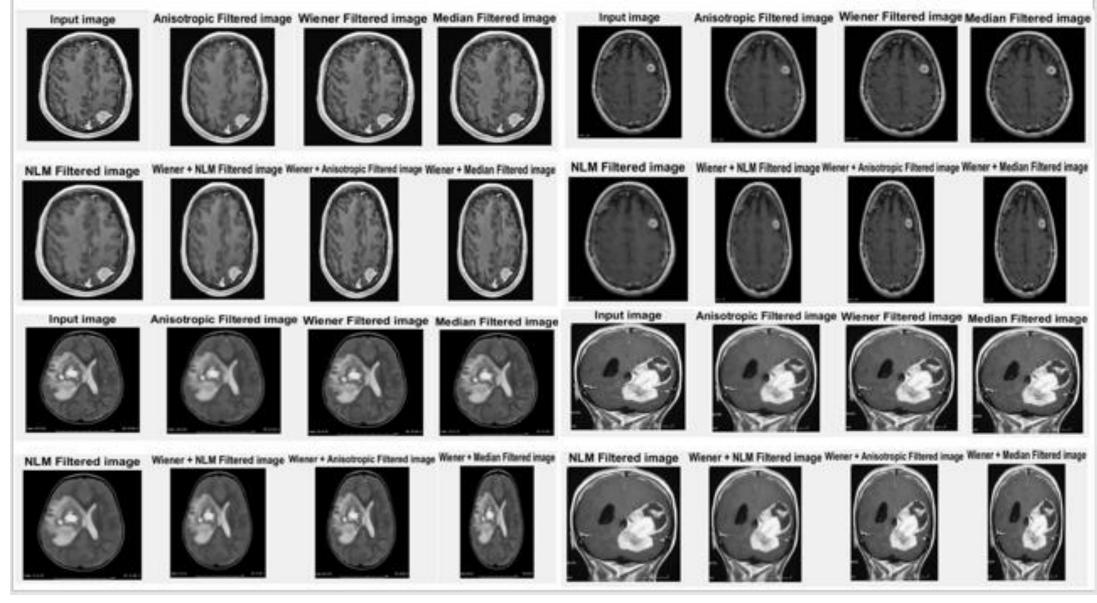


Figure-8: Implementation of different pre-processing filtering algorithms

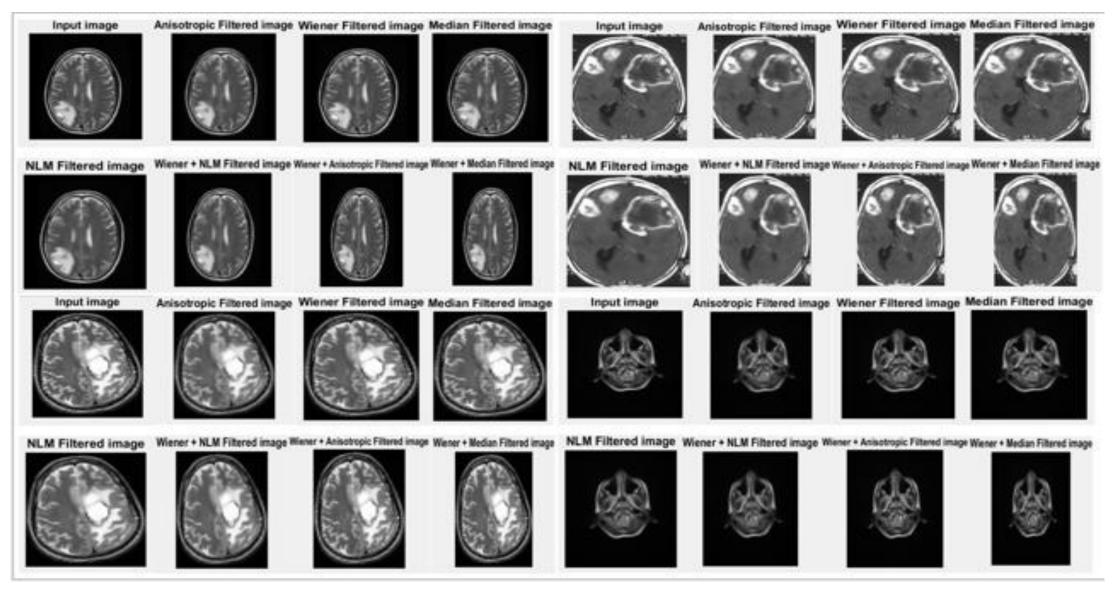


Figure-9: Implementation of different pre-processing filtering algorithms

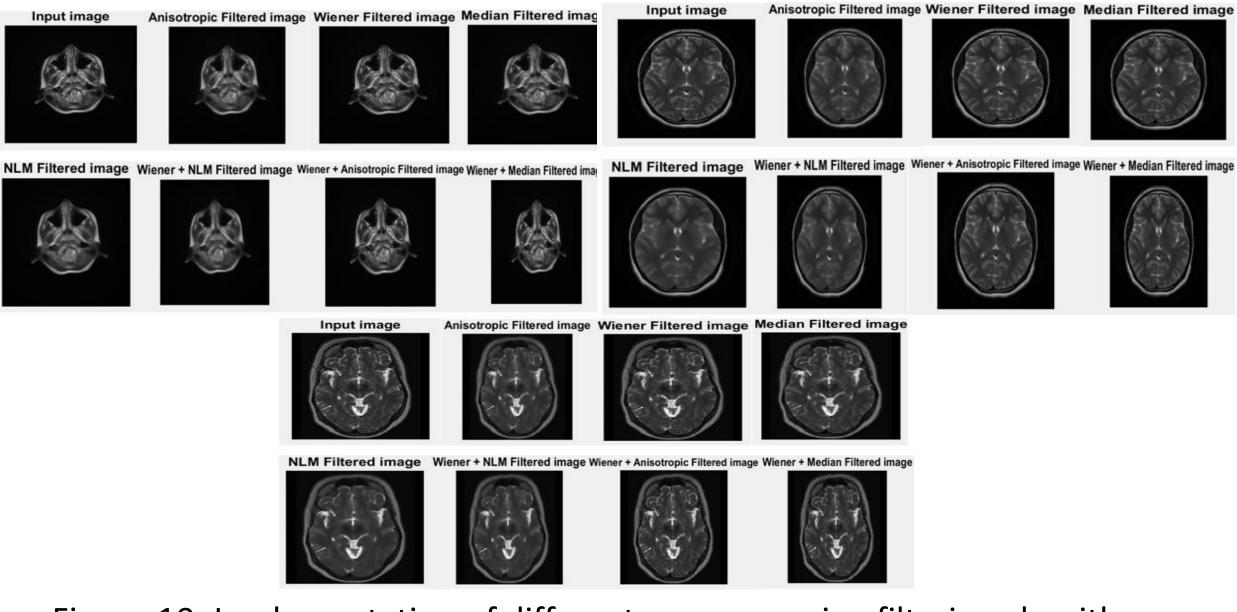


Figure-10: Implementation of different pre-processing filtering algorithms

3) Segmentation

Bi-level Thresholding

$$TH_0 = \{J(x, y) \in I : 0 \le J(x, y) \le th_1 - 1\}$$

$$TH_1 = \{J(x, y) \in I : th_1 \le J(x, y) \le L - 1\}$$

Multilevel Thresholding

$$\begin{array}{l} TH_0 = \{ J(x,y) \in I : 0 \leq J(x,y) \leq th_1 - 1 \} \\ TH_1 = \{ J(x,y) \in I : th_1 \leq J(x,y) \leq th_2 - 1 \} \\ TH_i = \{ J(x,y) \in I : th_i \leq J(x,y) \leq th_{i+1} - 1 \} \\ TH_r = \{ J(x,y) \in I : th_r \leq J(x,y) \leq L - 1 \} \end{array}$$

I - original MRI images, L - total number of distinct thresholding levels, J(x, y) - corresponding intensity value with respect to (x, y) coordinate, $th_i = 1, 2, \cdots$ L

> Cuckoo search algorithm:

Principal of the CS algorithm [53]: :

- 1. Each cuckoo bird lays one egg at a time and randomly places its egg in a host bird's nest.
- 2. The best nests containing high-quality eggs are carried over to the next generations.
- 3. The number of available host nests is fixed. The host bird discovers foreign eggs with a probability p_{α} , and the range of p_{α} is from 0 to 1. The best nests are selected for further calculations.

The CS process can be summarized as follows: While generating new solution x_i^{t+1} for cuckoo i, a Lévy flight is performed:

$$x_i^{t+1} = x_i^t + \alpha_0(x_i^t - x_{best}) \oplus Levy(\lambda)$$

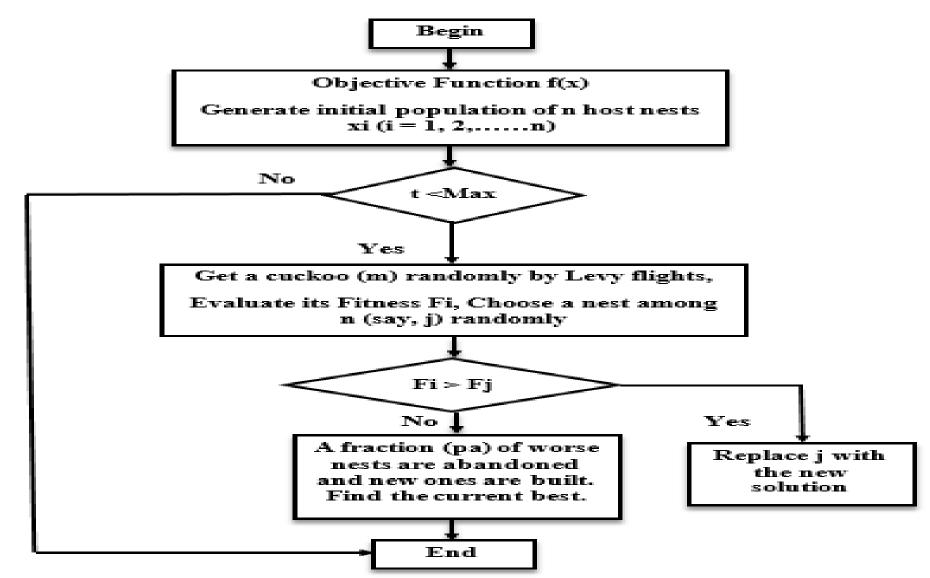
 α_0 - step scaling factor, x_{best} - current optimal solution

 \oplus - Element-wise multiplication

Levy flights are drawn from a Levy distribution, which can be defined by:

$$Levy(\lambda) \sim u = t^{-\lambda}, (1 < \lambda \le 3)$$

Flow Chart Of The Cuckoo Search Algorithm:



Objective functions1. Otsu's

- To optimize between-class variance by choosing an appropriate threshold value
- p_i probability of the pixel intensity value, i 0 to 255
- L total number of distinct intensity levels in the gray scale image

$$x_{best} = Arg \max\{\sigma_B^2(t)\}$$

$$\sigma_B^2 = \sigma_0^2 + \sigma_1^2 + \sigma_2^2 + \dots \sigma_r^2 \sigma_0^2 = \omega_0 (\mu_0 - \mu_T)^2 \sigma_1^2 = \omega_1 (\mu_1 - \mu_T)^2 \sigma_r^2 = \omega_r (\mu_r - \mu_T)^2$$

$$\omega_{0} = \text{weight} = \frac{\sum_{i=0}^{t_{1}-1} p_{i}}{\sum_{i=0}^{L-1} p_{i}} \qquad \qquad \omega_{1} = \text{weight} = \frac{\sum_{i=t_{1}}^{t_{2}-1} p_{i}}{\sum_{i=0}^{L-1} p_{i}}$$
$$\omega_{r} = \text{weight} = \frac{\sum_{i=t_{r}}^{L-1} p_{i}}{\sum_{i=0}^{L-1} p_{i}} \qquad \qquad \mu_{1} = \text{mean} = \frac{\sum_{i=t_{1}}^{t_{2}-1} i.p_{i}}{\sum_{i=t_{1}}^{t_{2}-1} p_{i}}$$
$$\mu_{r} = \text{mean} = \frac{\sum_{i=t_{r}}^{L-1} i.p_{i}}{\sum_{i=t_{r}}^{L-1} p_{i}} \qquad \qquad \mu_{T} = \text{mean} = \frac{\sum_{i=0}^{L-1} i.p_{i}}{\sum_{i=0}^{L-1} p_{i}}$$

2. Kapur Entropy

$$x_{best} = Arg \max\{H_T(t)\}$$

$$H_T = H_0 + H_1 + H_2 \dots + H_r$$

$$H_{0} = -\sum_{i=0}^{t_{1}-1} \frac{p_{i}}{w(0)} ln \frac{p_{i}}{w(0)}$$

$$H_{1} = -\sum_{i=t_{1}}^{t_{2}-1} \frac{p_{i}}{w(1)} ln \frac{p_{i}}{w(1)}$$

$$H_{2} = -\sum_{i=t_{2}}^{t_{3}-1} \frac{p_{i}}{w(1)} ln \frac{p_{i}}{w(2)}$$

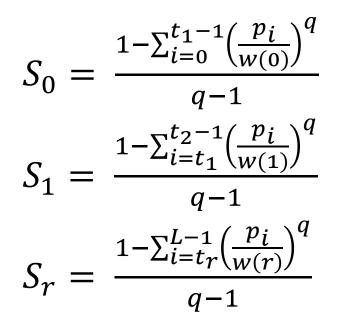
$$H_{r} = -\sum_{i=t_{r}}^{L-1} \frac{p_{i}}{w(r)} ln \frac{p_{i}}{w(r)}$$

$$w(0) = \sum_{i=0}^{t_1 - 1} p_i$$
$$w(1) = \sum_{i=t_1}^{t_2 - 1} p_i$$
$$w(2) = \sum_{i=t_2}^{t_3 - 1} p_i$$
$$w(r) = \sum_{i=t_m}^{L - 1} p_i$$

3. Tsallis Entropy

 $x_{best} = Arg \max\{S_T(t)\}$

 $S_T = S_0 + S_1 + S_2 \dots + S_r + (1 - q) \cdot (S_0 \cdot S_1 \cdot S_2 \dots \cdot S_r)$



$$w(0) = \sum_{i=0}^{t_1-1} p_i$$

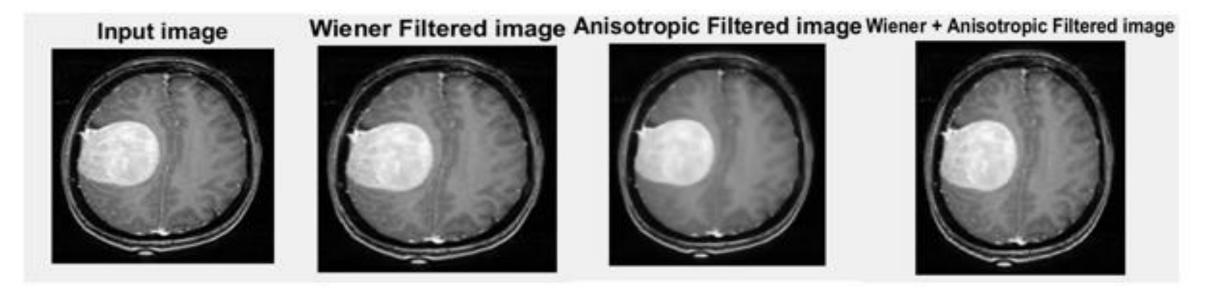
$$w(1) = \sum_{i=t_1}^{t_2-1} p_i$$

$$w(r) = \sum_{i=t_m}^{L-1} p_i$$

4. Combined Otsu with Tsallis Entropy

 x_{best} = $Arg max\{\mu(t)\}$

$$\mu(t) = S_T - (\sigma_B^2)^{1-q}$$



Cuckoo Otsu Thresholded Image Cuckoo Kapur Thresholded Image Cuckoo Tsallis Thresholded Image Cuckoo Combined Otsu and Tsallis Image



Figure-11: Implementation of different segmentation techniques

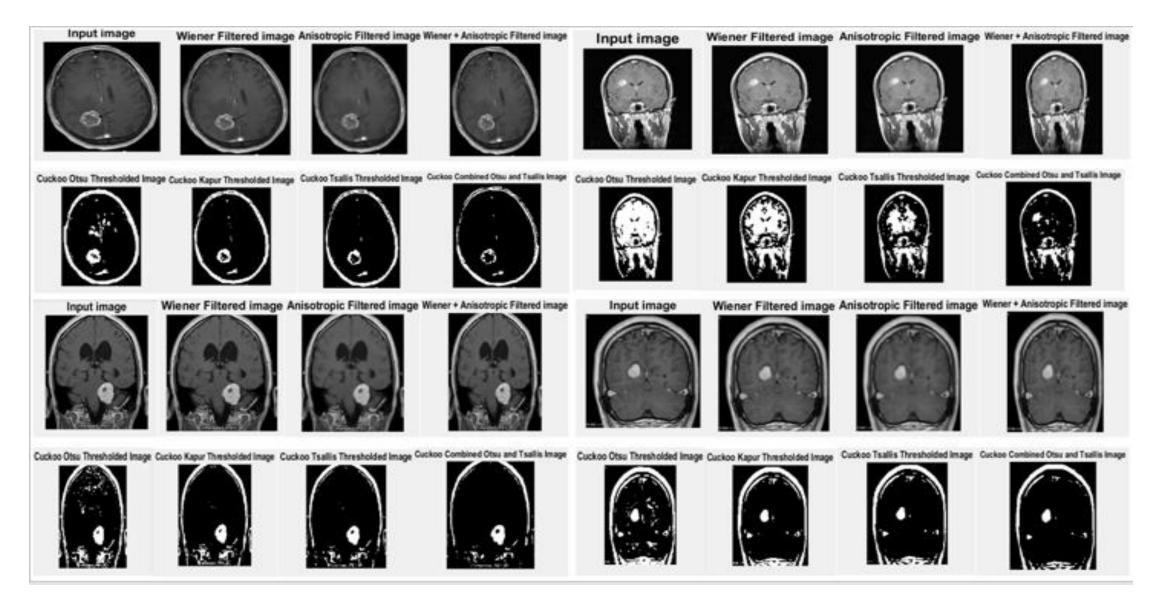


Figure-12: Implementation of different segmentation techniques

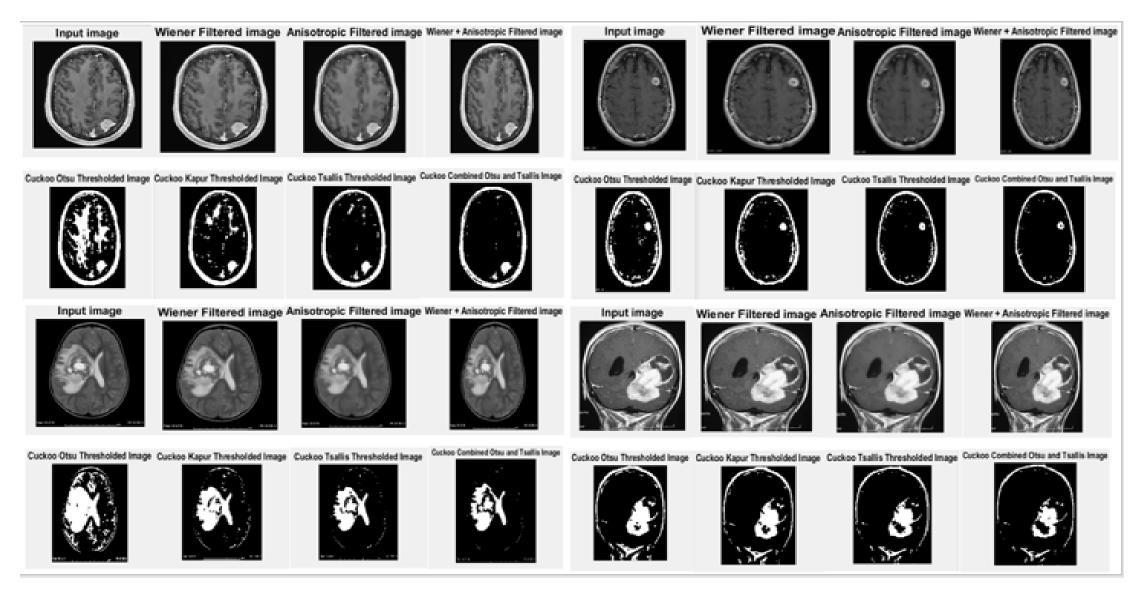


Figure-13: Implementation of different segmentation techniques

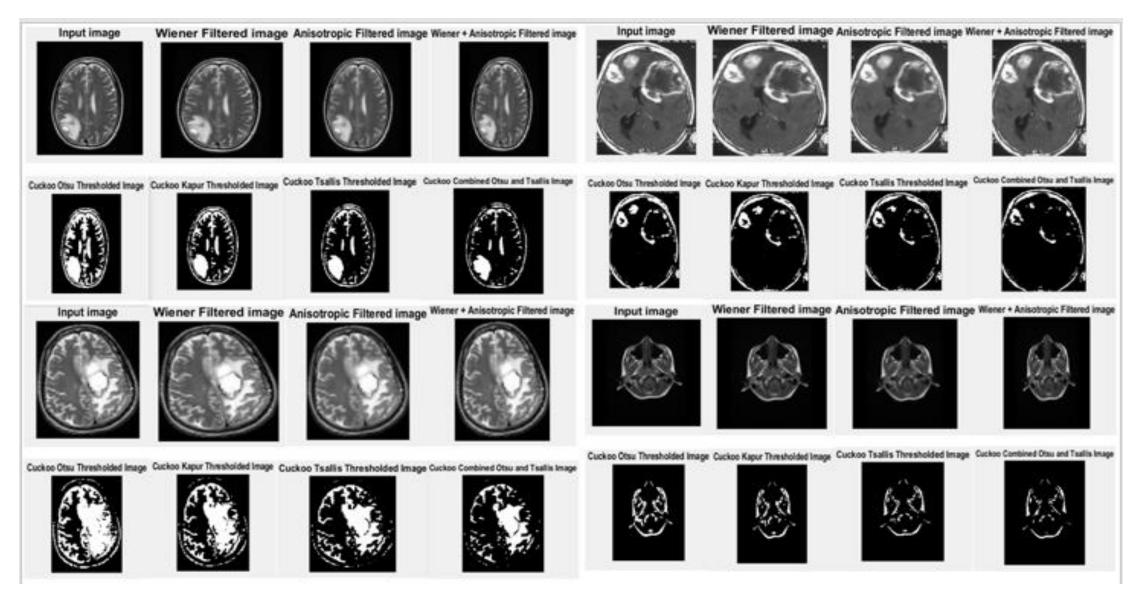


Figure-14: Implementation of different segmentation techniques

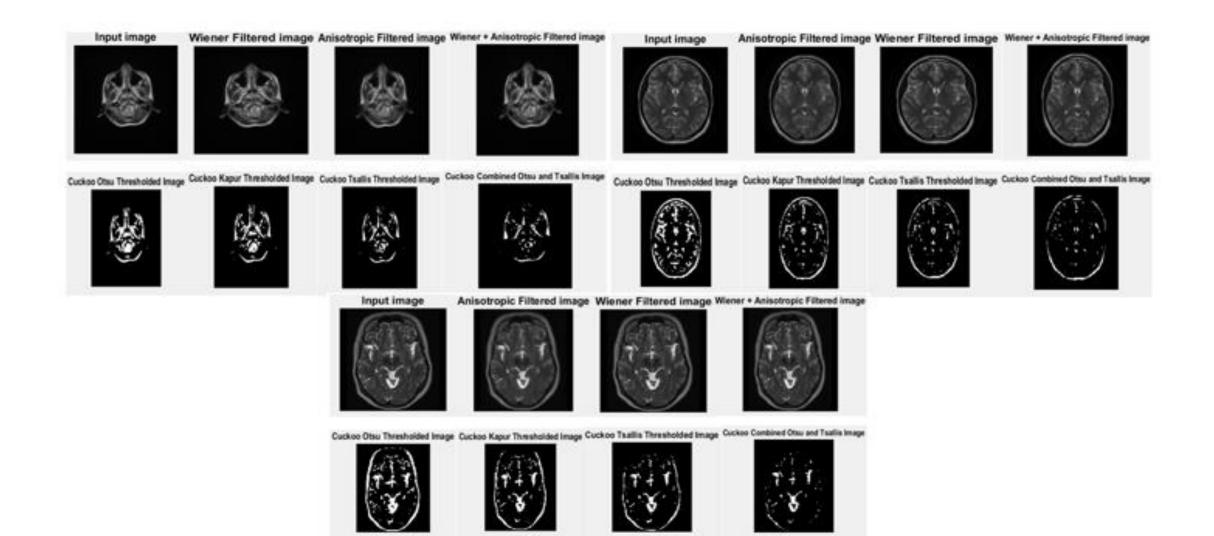


Figure-15: Implementation of different segmentation techniques

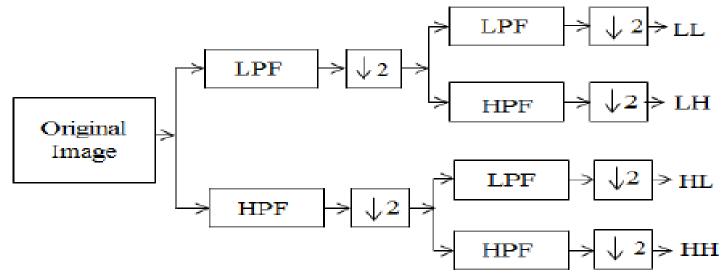
4) Feature Extraction

DWT works by applying a series of filters to the input signal or image, which separate it into low-frequency and high-frequency components. These components can then be further decomposed into sub-bands, creating a tree-like structure known as a wavelet decomposition.

The coefficients can be computed using filter banks, where the LL coefficients represent the low-frequency approximation and the remaining coefficients represent the high-frequency details in different directions.

- x(n) input signal or image,
- h(n) low-pass filter coefficients
- g(n) high-pass filter coefficients

The DWT equations for obtaining the LL, LH, HL, and HH coefficients can be written as follows:



$$LL(n) = x * h * h (downsampling by 2)$$

$$LH(n) = x * h * g (downsampling by 2)$$

$$HL(n) = x * g * h (downsampling by 2)$$

$$HH(n) = x * g * g (downsampling by 2)$$

• downsampling by 2 - reduces the size of the coefficients by half, * - convolution

Statistical Parameters

Image	Contrast	Correlation	Energy	Homogeneity	Mean	Standard Deviation
Image 1	0.2539	0.1014	0.7610	0.9329	0.0017	0.0892
Image 2	0.2258	0.1529	0.7689	0.9364	0.0017	0.0892
Image 3	0.2152	0.1143	0.7526	0.9326	0.0048	0.0896
Image 4	0.3167	0.1297	0.7949	0.9395	0.0075	0.0899
Image 5	0.243	0.0943	0.7488	0.9300	0.0050	0.0897
Image 6	0.23	0.0871	0.7513	0.9301	0.0046	0.0895
Image 7	0.2364	0.1479	0.7429	0.9287	0.0046	0.0895

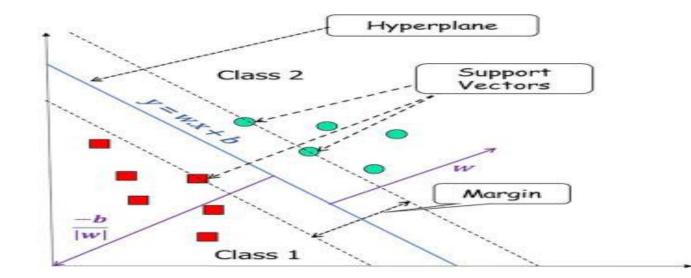
Figure-16: Statistical parameters (1 to 6) for different brain images

Image	Entropy	RMS	Variance	Kurtosis	Skewness	Inverse Different Moment
Image 1	2.9641	0.0898	0.0081	7.8474	0.5534	0.1548
Image 2	3.0447	0.0897	0.0082	7.2954	0.3964	0.6042
Image 3	3.7365	0.0868	0.0081	5.8455	0.4031	1.5651
Image 4	3.1611	0.0892	0.0080	13.499	1.3523	0.8302
Image 5	3.614	0.0892	0.0081	6.052	0.5247	1.1661
Image 6	3.7295	0.0848	0.0082	5.6958	0.3829	0.5801
Image 7	3.5494	0.0886	0.0081	6.573	0.6144	0.3837

Figure-17: Statistical parameters (7 to 12) for different brain images

5) Feature Classification

Support Vector Machine is used for classification. The basic idea behind SVM is to transform the input data into a higher-dimensional space, where it becomes easier to find a decision boundary that separates the different classes. This decision boundary is defined by a hyperplane that maximizes the margin between the two closest points from different classes. The points that lie on the margin are called support vectors, hence the name Support Vector Machines.



• 2×2 Confusion Matrix

Total Brain Images		Predicted		
		With Brain Tumor Without Brain		
Actual	With Brain Tumor	ТР	FN	
	Without Brain Tumor	FP	TN	

• 2×2 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Otsu as an Objective function

Total Brain Im	ages – 170	Predicted		
With Brain Tumo	r Images – 110	With Brain Tumor	Without Brain Tumor	
Without Brain Tu	mor Images - 60			
Actual	Actual With Brain Tumor		10	
	Without Brain Tumor	07	53	

• 2×2 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Kapur Entropy as an Objective function

Total Brain I	mages – 170	Predicted		
With Brain Tum	or Images – 110	With Brain Tumor	Without Brain Tumor	
Without Brain T	umor Images - 60			
Actual	With Brain Tumor	103	07	
	Without Brain Tumor	05	55	

• 2×2 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Tsallis Entropy as an Objective function

Total Brain Im	nages – 170	Predicted		
With Brain Tumo	r Images – 110	With Brain Tumor	Without Brain Tumor	
Without Brain Tu	mor Images - 60			
Actual	With Brain Tumor	106	04	
	Without Brain Tumor	04	56	

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 2×2 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Combined Otsu and Tsallis Entropy as an Objective function

Total Brain I	mages – 170	Predicted		
With Brain Tum	or Images – 110	With Brain Tumor	Without Brain Tumor	
Without Brain To	umor Images - 60			
Actual	With Brain Tumor	108	02	
	Without Brain Tumor	03	57	

• Performance evaluation statistical parameters

Negative Predictive Value (NPV) =
$$\frac{TN}{TN+FN}$$
Specificity $(S_p) = \frac{TN}{FP+TN}$ Positive Predictive Value (PPV) = $\frac{TP}{TP+FP}$ Sensitivity $(S_e) = \frac{TP}{TP+FN}$

$$Accuracy (Acc) = \frac{IP + IN}{TP + FN + TN + FP}$$

Parameters	Combined Wiener and Anisotropic Filter using CSA with Otsu as an Objective function	Combined Wiener and Anisotropic Filter using CSA with Kapur Entropy as an Objective function	Combined Wiener and Anisotropic Filter using CSA with Tsallis Entropy as an Objective function	Combined Wiener and Anisotropic Filter using CSA with Combined Otsu and Tsallis Entropy as an Objective function
Se	0.909	0.936	0.9636	0.981
Sp	0.8833	0.9166	0.9333	0.9500
PPV	0.9345	0.9537	0.9636	0.9729
NPV	0.8412	0.8870	0.9333	0.9661
Асс	0.900	0.929	0.952	0.970

Figure-18: Performance evaluation statistical parameters for brain tumor classification using 2×2 Confusion Matrix

• 3×3 Confusion matrix

Tota	Total Brain Images – 340 With Brain Tumor Images – 220		Predicted			
			With Malignant	Without Brain		
Without	Brain Tumor Images - 120	Brain Tumor	Brain Tumor	Tumor		
	With Benign Brain Tumor	Α	В	С		
Actual	With Malignant Brain Tumor	D	E	F		
	Without Brain Tumor	G	Н	I		

• 3×3 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Otsu as an Objective function

Total Brain Images – 340		Predicted		
With Brain Tumor Images – 220		With Benign	With Malignant	Without Brain
Without E	Brain Tumor Images - 120	Brain Tumor	Brain Tumor	Tumor
	With Benign Brain Tumor	120	06	04
Actual	With Malignant Brain Tumor	06	80	04
	Without Brain Tumor	08	06	106

• 3×3 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Kapur Entropy as an Objective function

Tota	Total Brain Images – 340		Predicted		
With B	With Brain Tumor Images – 220		With Malignant	Without Brain	
Without	Brain Tumor Images - 120	Brain Tumor	Brain Tumor	Tumor	
Actual	With Benign Brain Tumor	124	03	03	
Actual	With Malignant Brain Tumor	04	82	04	
	Without Brain Tumor	06	04	110	

• 3×3 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Tsallis Entropy as an Objective function

Tota	Total Brain Images – 340		Predicted			
With Bra	With Brain Tumor Images – 220		With Malignant	Without Brain		
Without I	Without Brain Tumor Images - 120		Brain Tumor	Tumor		
	With Benign Brain Tumor	127	01	02		
Actual	With Malignant Brain Tumor	03	85	02		
	Without Brain Tumor	05	03	112		

• 3×3 Confusion Matrix with Combined Wiener and Anisotropic Filter using Cuckoo Search Algorithm with Combined Otsu and Tsallis Entropy as an Objective function

	al Brain Images – 340		Predicted	
	rain Tumor Images – 220 Brain Tumor Images - 120	With Benign	With Malignant	Without Brain
		Brain Tumor	Brain Tumor	Tumor
	With Benign Brain Tumor	128	01	01
Actual	With Malignant Brain Tumor	01	88	01
	Without Brain Tumor	04	02	114

• TP, FP, TN, FN

А	В	С
D	E	F
G	Н	I

	Benign Tumor	Maligant Tumor	Without Tumor
ТР	Α	E	I
FP	D+G	B+H	C+F
TN	E+F+H+I	A+C+G+I	A+B+D+E
FN	B+C	D+F	G+H

	Combined Wiener and Anisotropic Filter using CSA with Otsu as an Objective function	Combined Wiener and Anisotropic Filter using CSA with Kapur Entropy as an Objective function	Combined Wiener and Anisotropic Filter using CSA with Tsallis Entropy as an Objective function	Combined Wiener and Anisotropic Filter using CSA with Combined Otsu and Tsallis Entropy as an Objective function
TP(Benign)	120	124	127	128
TP(Malignant)	80	82	85	88
TP(Without Tumor)	106	110	112	114
FP(Benign)	14	10	08	05
FP(Malignant)	12	07	04	03
FP(Without Tumor)	08	07	04	02
TN(Benign)	196	200	202	205
TN(Malignant)	238	243	246	247
TN(Without Tumor)	212	213	216	218
FN(Benign)	10	06	03	02
FN(Malignant)	10	08	05	02
FN(Without Tumor)	14	10	08	06

Figure-19: Different methods with TP, FP, TN and FN for Benign, Malignant tumor and without tumor 54

	Combined Wiener and	Combined Wiener and	Combined Wiener and	Combined Wiener and Anisotropic
Parameters	Anisotropic Filter using CSA with Otsu as an	Anisotropic Filter using CSA with Kapur Entropy	Anisotropic Filter using CSA with Tsallis Entropy	Filter using CSA with Combined Otsu and Tsallis Entropy as an
rataineters	Objective function	as an Objective function	as an Objective function	Objective function
	0.92308	0.95385	0.97692	0.98462
Se(Benign Tumor)	0.88889	0.91111	0.94444	0.97778
Se(Malignant Tumor)				
Se(Without Tumor)	0.88333	0.91667	0.93333	0.95000
Sp(Benign Tumor)	0.93333	0.95238	0.96190	0.97619
Sp(Malignant Tumor)	0.95200	0.97200	0.98400	0.98800
Sp(Without Tumor)	0.96363	0.96818	0.98181	0.99090
PPV(Benign Tumor)	0.89552	0.92537	0.94074	0.96241
PPV(Malignant Tumor)	0.86957	0.92135	0.95506	0.96703
PPV(Without Tumor)	0.92982	0.94017	0.96552	0.98276
NPV(Benign Tumor)	0.95145	0.97087	0.98536	0.99033
NPV(Malignant Tumor)	0.95967	0.96812	0.98000	0.99196
NPV(Without Tumor)	0.93805	0.95515	0.96428	0.97321
ACC(Benign Tumor)	0.92941	0.95294	0.96764	0.97941
ACC(Malignant Tumor)	0.93529	0.95588	0.97352	0.98529
ACC(Without Tumor)	0.93529	0.95000	0.96470	0.97647
ACC(all)	0.90000	0.92941	0.95294	0.97059

Figure-20: Performance evaluation statistical parameters for brain tumor classification using 3×3 Confusion Matrix

6) GUI Implementation

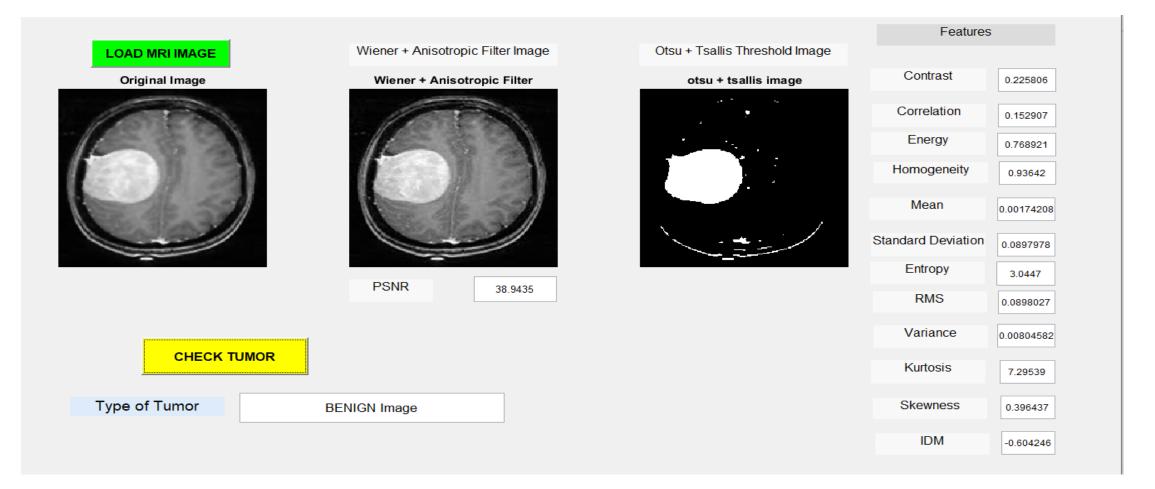


Figure-21: GUI Implementation of the tumor classification for Image-1

			Features				Features	i
LOAD MRI IMAGE	Wiener + Anisotropic Filter Image	Otsu + Tsallis Threshold Image		LOAD MRI IMAGE	Wiener + Anisotropic Filter Image	Otsu + Tsallis Threshold Image		
Original Image	Wiener + Anisotropic Filter	otsu + tsallis image	Contrast 0.265851	Original Image	Wiener + Anisotropic Filter	otsu + tsallis image	Contrast	0.25
			Correlation 0.110749				Correlation	0.118526
			Energy 0.76026	0.1	(Days)		Energy	0.754805
E 11 3	E-11-3		Homogeneity 0.933148				Homogeneity	0.931123
0	0	N O J	Mean 0.0026831	The second	1.12-14-10		Mean	0.00084736
			Standard Deviation 0.0897746				Standard Deviation	0.0898107
	PSNR 38 3534		Entropy 3.306	ROW IN	1994 A.		Entropy	2.62703
	PSNR		RMS 0.0898027		PSNR 35.5394		RMS	0.0898027
			Variance 0.00805014				Variance	0.00805376
	IOR		Kurtosis 8.03691	CHECK TUMOR			Kurtosis	7.14686
Type of Tumor	BENIGN Image		Skewness 0.871164	Type of Tumor	BENIGN Image		Skewness	0.568073
			IDM 1.19274				IDM	0.206125

Figure-22: GUI Implementation of the tumor classification for different images

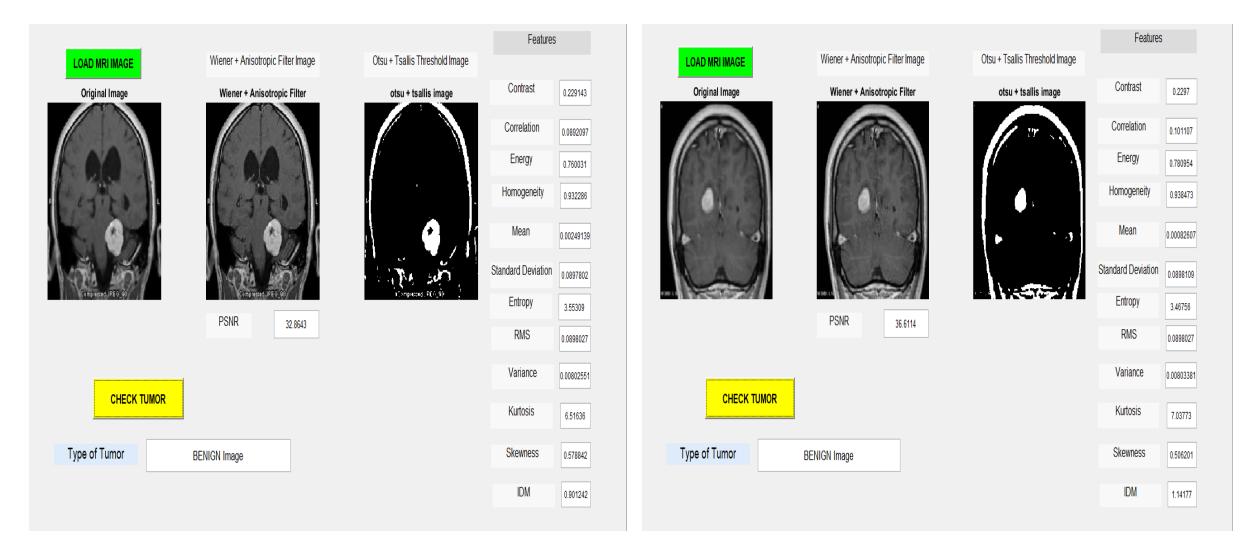


Figure-23: GUI Implementation of the tumor classification for different images

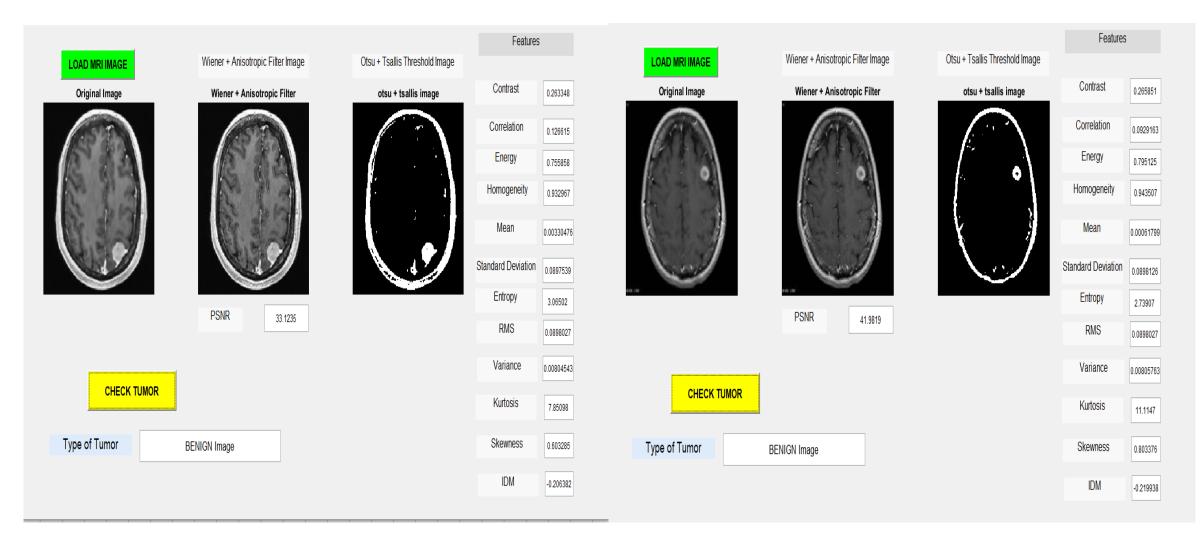


Figure-24: GUI Implementation of the tumor classification for different images

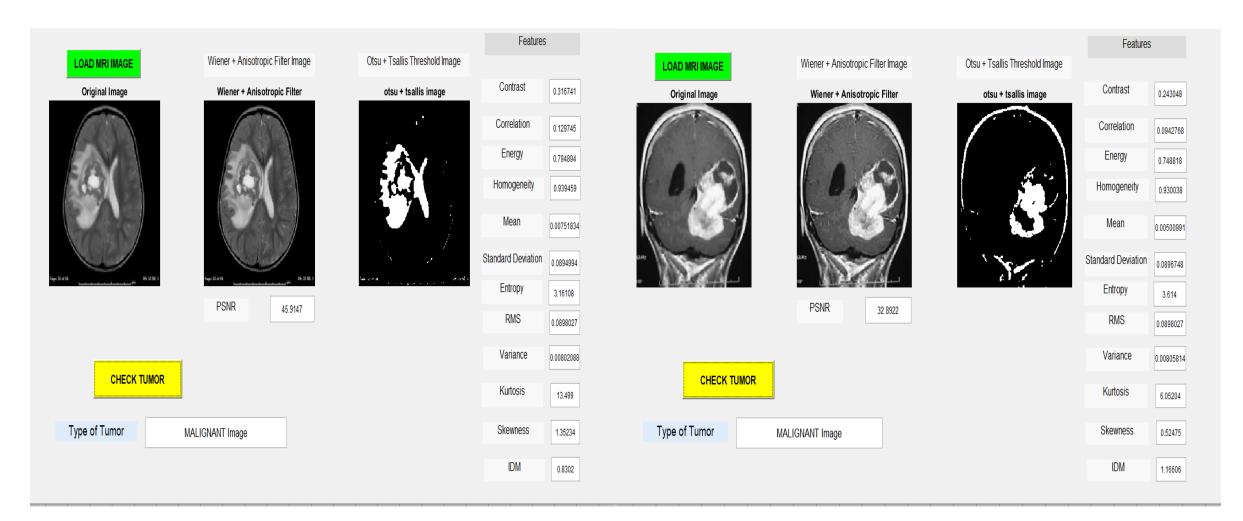


Figure-25: GUI Implementation of the tumor classification for different images

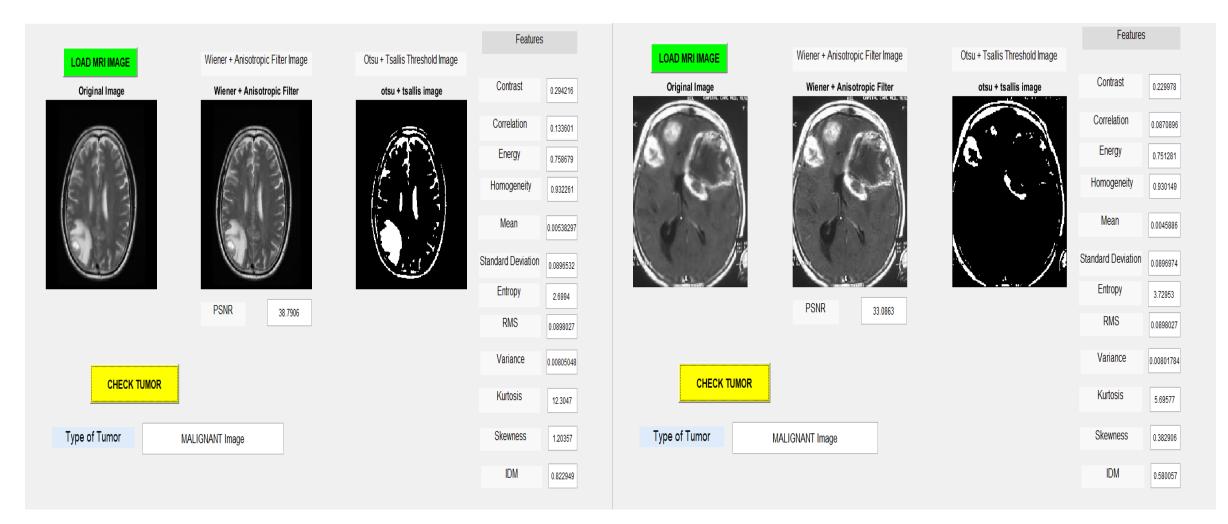


Figure-26: GUI Implementation of the tumor classification for different images



Figure-27: GUI Implementation of the tumor classification for different images



Figure-28: GUI Implementation of the tumor classification for different images



Figure-29: GUI Implementation of the tumor classification for different images

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7) CONCLUSION

- Dataset Online kaggle dataset (www.kaggle.com) and Patients data from Sahyog Imaging Centre, SSG Hospital
- Pre-Processing Wiener filter, Anisotropic filter, Median filter, Non-Local Means filter and Combined filters
 - Parameters Peak Signal to Noise Ratio, Mean Square Error, Root Mean Square Error and Universal Quality Index
 - Combined Wiener and Anisotropic used for next stage.

Segmentation - Cuckoo Search algorithm using different objective functions – Otsu's, Kapur Entropy, Tsallis Entropy, Combined Otsu's and Tsallis Entropy

For Feature extraction – Discrete Wavelet Transform

 Feature matrix is generated using twelve different parameters. Twelve statistical parameters covered are Contrast, Correlation, Energy, Homogeneity, Mean, Standard Deviation, Entropy, Root Mean Square, Variance, Kurtosis, Skewness and Inverse Different Moment

Classification – Support vector machine

- 2×2 and 3×3 confusion matrix
- Statistical parameters Sensitivity, Specificity, Positive Predictive Value, Negative Predictive Value and Accuracy
 - 2×2 confusion matrix With Tumor or Without Tumor
 - 3×3 confusion matrix Benign Tumor, Malignant Tumor and Without Tumor
- Cuckoo Search algorithm using Combined Otsu's and Tsallis Entropy gives better results compare to other algorithms.

8) FUTURE SCOPE

- > Research work can be extended with following possibilities:
 - More enhancement can be expressed with converting 2D data into 3D volumetric data
 - More optimization can be achieved with trial of different hybrid algorithms

9) PUBLICATIONS

CONFERENCE PAPERS

- B. K. Pancholi and P. S. Modi, "Noise reduction in Clinical MRI Scans employing Filter Combining Techniques," 2022 2nd International Conference on Technological Advancements in Computational Sciences (ICTACS), Tashkent, Uzbekistan, 2022, pp. 474-480, doi: 10.1109/ICTACS56270.2022.9988482, ISBN : 978-1-6654-7658-4, EISBN : 978-1-6654-7657-7
- B. K. Pancholi, P. S. Modi and N. G. Chitaliya, "A Review of Noise Reduction Filtering Techniques for MRI Images", 5th International Conference on Contemporary Computing and Informatics (IC3I-2022), Amity University, Greater Noida, Uttar Pradesh, pp. 954 - 960, doi: 10.1109/IC3I56241.2022.10073389, ISBN : 979-8-3503-9827-4, EISBN:979-8-3503-9826-7

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PATENT

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